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(21) International Application Number: PCT/US99/30118 (22) International Filing Date: 16 December 1999 (16.12.99) (30) Priority Data: 09/219,092 22 December 1998 (22.12.98) US (71) Applicant: ANGIOTRAX, INC. [US/US]; 743 N. Pastoria Avenue, Sunnyvale, CA 94086 (US). (72) Inventors: SAADAT, Vahid; 1 Avocet Drive, #204, Redwood Shores, CA 94065 (US). KERMODE, James; 1080 Kildare Avenue, Sunnyvale, CA 94087 (US). REAM, John, H.; 249 Omira Drive, San Jose, CA 95123 (US). (74) Agents: PISANO, Nicola, A. et al.; Fish & Neave, 1251 Avenue of the Americas, New York, NY 10020 (US).		(81) Designated States: AU, CA, JP, European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE). Published <i>With international search report.</i> <i>Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i>
(54) Title: METHODS AND APPARATUS FOR PERFUSING TISSUE AND/OR STIMULATING REVASCULARIZATION AND TISSUE GROWTH <div data-bbox="527 1113 1096 1543" data-label="Image"> </div> (57) Abstract <p>Apparatus and methods are provided for forming a channel in an organ or vessel to enhance perfusion therein. The apparatus may include a bioactive agent to stimulate tissue growth and vascularization in tissue adjacent to the channel. The apparatus includes a stent (10), suitable for percutaneous or intraoperative placement, that has a tubular member (12) with a plurality of tines (76, 82), barbs (60), ribs (113) or other structure to secure the stent at a desired position within tissue.</p>		

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METHODS AND APPARATUS FOR PERFUSING TISSUE
AND/OR STIMULATING REVASCULARIZATION
AND TISSUE GROWTH

Field Of The Invention

5 The present invention relates to apparatus
and methods for perfusing myocardial tissue and
stimulating tissue growth and revascularization in a
vessel or organ. More particularly, the present
invention relates to a device that may be implanted in
10 a vessel or organ, such as the heart, to form a channel
for perfusing tissue, and may include a bioactive agent
to stimulate tissue regeneration and vascularization.

Background Of The Invention

15 A leading cause of death in the United States
and the world today is coronary artery disease, in
which atherosclerotic plaque causes blockages in the
coronary arteries, resulting in ischemia of the heart
(i.e., inadequate blood flow to the myocardium). The
20 disease manifests itself as chest pain or angina. In
1996, approximately 7 million people suffered from
angina in the United States.

Coronary artery bypass grafting (CABG), in
which the patient's chest is surgically opened and an
25 obstructed artery replaced with a native artery
harvested elsewhere or a synthetic graft, has been the
conventional treatment for coronary artery disease for
the last thirty years. Such surgery creates
significant trauma to the patient, requires long
30 recuperation time, and poses serious risks of

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mortality. In addition, experience has shown that the bypass vessel or graft becomes obstructed with time, requiring further surgery.

More recently, catheter-based therapies such as percutaneous transluminal coronary angioplasty (PTCA) and atherectomy have been developed. In PTCA, a mechanical dilatation device is disposed across an obstruction in the patient's artery and then dilated to compress the plaque lining the artery to restore patency to the vessel. Atherectomy involves using a catheter having a mechanical cutting tip or a laser to cut (or ablate) a passage through the blockage. Such methods have drawbacks, however, ranging from re-blockage of vessels dilated by angioplasty, to catastrophic rupture or dissection of the vessel during atherectomy. Moreover, these methods only may be used for that fraction of the patient population that have a few, easily accessible blockages. Neither technique is suitable for the treatment of diffuse atherosclerosis.

A more recent experimental technique for treating ischemia uses recombinant protein therapy to induce neoangiogenesis in the human heart. Schumacher et al., Induction of Neoangiogenesis in Ischemic Myocardium by Human Growth Factors, 97 Circulation 645 (1998) report the results of a study in which fibroblast growth factor (FGF-I), a human growth factor obtained through genetic engineering, was injected into the myocardium of 20 patients suffering from stenosis of the internal mammary artery/left anterior descending coronary artery. Within 4 days after application of FGF-I, new capillary vessels radiated outward from the injection point. Although the results of the study appear encouraging, it is unclear whether growth factor therapy alone will be able to treat occlusions of the

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greater coronary vessels.

Another recent technique that holds promise of treating a large percentage of the patient population, including those patients suffering from
5 diffuse atherosclerosis, is referred to as transmyocardial revascularization (TMR). In this method, a series of channels are formed in the left ventricular wall of the heart. The channels may be transmural (i.e., from the epicardium to the
10 endocardium), or intramural (for example, from the endocardium and terminating in the myocardium).

Typically, between 15 and 40 channels about 1 mm in diameter and up to 3.0 cm deep are formed with a laser in the wall of the left ventricle to
15 perfuse the heart muscle with blood coming directly from the inside of the left ventricle, rather than from the coronary arteries. Apparatus and methods have been proposed to create these channels both percutaneously and intraoperatively (i.e., with the chest opened).

20 U.S. Patent Nos. 5,380,316 and 5,554,152 to Aita et al. describe intraoperative laser apparatus for forming channels extending from the epicardium to the endocardium. The laser includes an optical wave guide that is held against the patient's heart. Several
25 pulses of the laser are required to form a transmural channel by ablation. U.S. Patent No. 5,389,096 to Aita et al. describes a catheter-based laser system for performing TMR percutaneously, i.e., from within the left ventricle. U.S. Patent No. 4,658,817 to Hardy
30 describes a laser-based system for intraoperatively performing TMR that includes a needle portion for perforating an outer portion of the tissue, and a laser for ablating the inner portion.

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U.S. Patent No. 5,591,159 to Taheri describes a mechanical catheter-based apparatus for performing TMR involving a catheter having an end effector formed from a plurality of spring-loaded needles.¹ The catheter first is positioned percutaneously within the left ventricle. Then, a plunger is released so that the needles are thrust into the endocardium, and the needles are withdrawn, thus forming small channels that extend into the myocardium. The patent suggests that the needles may be withdrawn and advanced repeatedly at different locations under fluoroscopic guidance.

Although TMR has been observed to benefit many patients, researchers do not agree upon the mechanism by which TMR provides therapeutic benefits. One theory proposes that TMR channels remain patent for long periods of time, and provide a path by which oxygenated blood perfuses the myocardium. Relatively recent histological studies, however, indicate that TMR channels may close within a short time following the procedure. Fleischer et al., One-Month Histologic Response Of Transmyocardial Laser Channels With Molecular Intervention, 62 Ann. Soc. Thoracic Surg. 1051-58 (1996), describe a study that evaluated the histologic changes associated with laser TMR in a 1-month nonischemic porcine model, and report that the researchers were unable to demonstrate channel patency 28 days after TMR.

Patent Cooperation Treaty Publication No. WO 97/32551 describes apparatus for performing TMR that creates a TMR channel and then implants a stent in the channel to maintain channel patency. For intraoperative TMR, a needle obturator first creates a channel in the myocardium, and a stent is then inserted in the channel. For percutaneous TMR, a drill at the

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end of a catheter first forms channels in the myocardium, and then a stent is inserted into the channel.

The foregoing apparatus have the disadvantage
5 of requiring separate needle obturators or drills that must first create the channel before the stent is inserted into the myocardium. It therefore would be desirable to provide TMR stent apparatus to maintain channel patency, but that does not require a separate
10 channel forming device.

An alternative theory regarding the means by which TMR provides therapeutic benefits proposes that in addition to channel formation and patency, myocardial neovascularization outside the channel area
15 following channel formation is also important. To investigate this theory, researchers have combined the techniques of TMR and neoangiogenesis to study the use of gene therapy to promote blood vessel growth in the tissue surrounding laser TMR channels. In one study,
20 researchers intraoperatively administered a single dose of vascular endothelial growth factor (VEGF) within the channels formed by laser TMR. While no significant increase in myocardial vascularity was observed, it was hypothesized that increased residency of VEGF may be
25 required to stimulate angiogenesis.

Because the therapeutic benefit of TMR may result from a combination of channel patency and myocardial angiogenesis outside the channel area, it also would be desirable to provide methods and
30 apparatus that maintain TMR channel patency and stimulate neoangiogenesis in the myocardial tissue surrounding TMR channels.

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Summary Of The Invention

In view of the foregoing, it is an object of this invention to provide apparatus and methods for simultaneously forming a channel within a vessel or organ and introducing a stent to retain that channel patent, without requiring the use of a separate channel forming device.

It is a further object of the present invention to provide apparatus and methods comprising an implantable device that maintains channel patency and that may include a bioactive agent to stimulate tissue growth and revascularization.

It is a further object of this invention to provide apparatus and methods for implanting a series of stents at a plurality of tissue locations without having to repeatedly reload the stent delivery system.

These and other objects of the present invention are accomplished by providing a stent that simultaneously creates a channel in a vessel or organ and becomes implanted therein, to maintain the patency of the channel. The stent preferably includes a first end region that forms an intramural channel, and means for retaining the stent within the channel, such as an expandable mesh portion, barbs, tines or ribs, so that it is not dislodged by heart wall motion. The stent may comprise a bioactive agent to stimulate tissue regeneration and/or vascularization in tissue adjacent to the stent following implantation.

In one embodiment, the stent is configured from implantation in the left ventricle to promote perfusion and angiogenesis. The stent preferably includes a bore having an inlet, an outlet, and a plurality of apertures that extend from the bore to an exterior lateral surface of the stent. The stent may

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be fabricated from a bioresorbable material impregnated with a bioactive agent, such as an angiogenic growth factor, or alternatively, from nonresorbable material coated with a layer of a bioactive agent.

5 The stent optionally may include a second end region having means for securing the stent against movement, such as a flange, or one or more self-expanding barbs or tines. In other embodiments the stent may comprise a series of conical ribs or conical
10 sections formed of a bioresorbable material impregnated with a bioactive agent, or may include bioactive agents that vary as a function of length or thickness of the stent. In yet other embodiments, the stent may comprise a rod of bioresorbable material that is
15 implanted intraoperatively adjacent to a constricted artery to stimulate revascularization.

Delivery systems and methods of use are also provided for simultaneously forming a channel in a vessel or organ, and implanting the stent.

20 Brief Description Of The Drawings

Further features of the invention, its nature and various advantages will be more apparent from the accompanying drawings and the following detailed
25 description of the preferred embodiments, in which:

FIG. 1 is a side view of a first embodiment of a stent in its unexpanded state constructed in accordance with the present invention;

FIG. 2 is a side view of the stent of FIG. 1
30 in its expanded state;

FIG. 3 is a sectional view along line 3--3 of FIG. 1;

FIGS. 4A and 4B are, respectively, a view of an illustrative delivery system for use in implanting
35 the stent of FIG. 1 and a sectional side view of a

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distal end of the delivery system of FIG. 4A and the stent of FIG. 1;

FIG. 5 is a side view of the stent of FIG. 1 at an interval following implantation;

5 FIGS. 6A and 6B are, respectively, a side view and a sectional view, along line 6B--6B of FIG. 6A, of an alternative embodiment of a stent constructed in accordance with the present invention;

10 FIGS. 7A and 7B are, respectively, a perspective view and end view, along view line 7B--7B, of an alternative embodiment of a stent of the present invention in a contracted delivery state;

 FIGS. 8A and 8B are, respectively, a perspective view and end view, along view line 8B--8B, 15 of the stent of FIGS. 7A and 7B, in a deployed state;

 FIG. 9 is a perspective view of a further alternative embodiment of a stent constructed in accordance with the principles of the present invention;

20 FIG. 10 is a perspective view of still another alternative embodiment of a stent constructed in accordance with the principles of the present invention, in a deployed state;

 FIGS. 11A and 11B are, respectively, a side 25 view and an end view of a further alternative embodiment of a stent constructed in accordance with the present invention;

 FIGS. 12A and 12B are, respectively, a view of another illustrative delivery system and a sectional 30 side view of a distal end of that delivery system;

 FIG. 13 is a side view of a further alternative embodiment of a stent constructed in accordance with the present invention;

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FIGS. 14A and 14B are side views of still another embodiment of a stent constructed in accordance with the present invention in a contracted delivery state and deployed state, respectively;

5 FIGS. 14C and 14D are, respectively, side and end views of a component suitable for use in the stent of FIGS. 14A and 14B; and

FIG. 15 is a perspective view illustrating a method of implanting yet another embodiment of a stent
10 of the present invention to stimulate revascularization.

Detailed Description Of The Invention

The present invention relates generally to
15 apparatus and methods for forming a channel in a wall of a vessel or organ and implanting a stent that perfuses the tissue. In addition, the stent may include a bioactive agent to stimulate revascularization and/or tissue growth, such as
20 vascular endothelial growth factor (VEGF), e.g., VEGF165 or VEGF121, fibroblast growth factor, type I (FGF-I) or type II (FGF-II), PDGF, MCPI, platelet components, cardio myocytes or endothelial cells. The following written description describes illustrative
25 embodiments of the present invention, delivery systems for use therewith, and describes operation of such systems. Features suitable for use in further alternative embodiments also are set forth.

Although the invention is described
30 hereinafter as particularly useful in the emerging field of transmyocardial revascularization, methods and apparatus in accordance with the present invention advantageously may be used for perfusing or stimulating tissue regeneration in other organs and vessels. In
35 addition, although the present invention describes

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using bioactive agents, such as angiogenic growth factors, for stimulating myocardial revascularization, the methods and apparatus of the present invention also may be used for providing other drugs, proteins and
5 bioactive agents.

Referring to FIGS. 1 and 2, illustrative apparatus 10 constructed in accordance with the present invention is described. In FIG. 1, stent 10 comprises tubular body 12, having exterior surface 14, flange 16
10 extending radially outward from exterior surface 14, sharpened tip 18, and expandable mesh structure 20. Body 12 includes a bore and a plurality of apertures 22 that extend from the bore to exterior lateral surface 14 of the stent. In FIG. 2 stent 10 is shown
15 with expandable mesh structure 20 in its expanded state, for example, as the stent may be implanted in the myocardium of the left ventricle.

Referring now also to FIG. 3, the internal structure of stent 10 is described. Bore 24 extends
20 from flange 16 to sharpened tip 18, and permits fluid communication between the interior and exterior surface 14 of the stent 10 via apertures 22. In particular, blood from the left ventricle enters bore 24 through an inlet at flange 16, flows through the bore toward
25 sharpened tip 18, and exits through apertures 22 to supply blood to tissue within which the stent is implanted. Although FIG. 3 illustrates symmetrically opposed apertures 22, it will be understood that one or more apertures may be included without departing from
30 the principles of the present invention.

Tubular body 12 may be fabricated from metal, plastic, or a bioresorbable material. Suitable metals include, for example, stainless steel, nickel, nickel titanium, and tantalum, whereas suitable plastic

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materials include polyetheretherketone (PEEK), polysulfone, and polyimide. Hydroxyapatite, polyglycolic acid and polylactic acid are examples of bioresorbable materials that may be advantageously used
5 to construct tubular body 12.

In accordance with one aspect of the present invention, stent 10 may be coated on either interior surface 26 or exterior surface 14 with a layer of bioactive agent 28, such as a drug or angiogenic growth
10 factor. Suitable growth factors may comprise, for example, vascular endothelial growth factor (VEGF), e.g., VEGF165 or VEGF121, fibroblast growth factor, type I (FGF-I) or type II (FGF-II), PDGF, MCP1, platelet components, cardio myocytes or endothelial
15 cells.

Applicants expect that if coating 28 is disposed on exterior surface 14 of stent 10, sustained exposure by the tissue to the bioactive agent will stimulate revascularization and/or tissue regeneration
20 in the tissue surrounding the stent. Alternatively, if coating 28 is disposed on interior surface 26 of bore 24, it is expected that the bioactive agent will be dissolved by blood entering bore 24, and carried into tissue surrounding stent 10 through apertures 22.
25 As further alternatives, stent 10 may be constructed from a bioresorbable material that is impregnated with a bioactive agent, or may be constructed from nonresorbable material coated with bioresorbable material that contains a bioactive agent.

30 Referring now to FIGS. 4A and 4B, illustrative delivery system 30 for forming a channel in tissue and implanting the stent of FIG. 1 is described. Delivery system 30 includes catheter 31 having distal end 32, first handle portion 33, push

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tube 34 and second handle portion 35. Second handle portion 35 includes syringe 36, which is coupled through lumen 37 (see FIG. 4B) to balloon element 38 disposed on the distal end of push tube 34.

5 Delivery system 30 may in addition include a series of stabilization members, such as described in copending commonly assigned U.S. patent application Serial No. 08/863,877, or U.S. Patent No. 4,813,930 to Elliott, both of which are incorporated herein by
10 reference. Such stabilization members may be desirable to counteract reaction forces generated during the implantation process as the stent is urged into the tissue.

 Push tube 34 is mounted for translation
15 through lumen 39 of catheter 31, and has push block 40 mounted near its distal end. Push block 40 abuts against the proximal face of flange 16 of stent 10. Balloon element 38 is disposed near the distal end of push tube 34 so that when the push tube is inserted
20 within bore 24 of stent 10, the balloon element is disposed within expandable mesh portion 20. Balloon element 38 is inflated via a suitable inflation medium using syringe 36 and lumen 37. Push tube 34 may comprise, for example, a stainless steel hypotube,
25 while balloon 38 preferably is non-compliant or semi-compliant, and may be constructed of polyethyl-tetraphlate, polyurethane or nylon. Balloon 38 is bonded to push tube 34 using techniques that are per se known.

30 Catheter 31 is of a length suitable for percutaneous transluminal deployment of stent 10, and may be constructed of materials conventionally used in manufacturing catheter systems, such as polyethylene, nylon or polyurethane. Alternatively, delivery system

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30 may be made much shorter, for example, if stents 10 are to be implanted intraoperatively, for example, through a surgical opening in the vena cava or aorta.

Delivery system 30 may be percutaneously and
5 transluminally inserted into the left ventricle using techniques that are per se known. During insertion of delivery system 30 to a treatment site, delivery system 30 is manipulated using first handle portion 33, while second handle portion 35 is in the proximal-most
10 position. Once distal endface 41 of catheter 31 has been disposed at an implantation site, for example, as determined by fluoroscopy, second handle portion 35 is translated towards first handle portion 33.

Movement of second handle portion 35 towards
15 first handle portion 33 (which is held stationary) urges push tube 34 in the distal direction. This translation is transmitted to push block 40 mounted on push tube 34, thereby causing stent 10 to extend from within lumen 39 and to pierce and become implanted in
20 the tissue. Forward movement of stent 10 into the myocardium is arrested when flange 16 abuts against the endocardium. Syringe 36 of second handle portion 35 is then actuated to expand balloon element 38, which turn deforms expandable mesh portion 20 to the state shown
25 in FIG. 2, for example, up to two times its original diameter. Syringe 36 is then withdrawn to collapse balloon element 38, and push tube 34 and catheter 31 are withdrawn.

In FIG. 5, stent 10 is described at an
30 interval of time after implantation. As shown in FIG. 5, stent 10 is implanted in myocardium M so that flange 16 abuts against endocardium E, and a plurality of vessels V have formed in a regenerated tissue layer T adjacent to the stent. Expandable mesh portion 20

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secures stent 10 within myocardium M, while flange 16 prevents the stent from being urged further into the myocardium due to the rhythmic contraction of the heart. It is expected that bore 24 of stent 10 will
5 preserve the patency of the channel, while apertures 22 will assist in perfusing the newly formed vasculature.

As an alternative to the above-described embodiment, expandable mesh portion 20 of stent 10 may instead be formed of a material, such as nickel-
10 titanium, so that mesh portion 20 self-expands when released from a restraint. Thus, for example, instead of deforming expandable mesh portion 20 using balloon element 38 as described hereinabove, stent 10 may instead be constrained within catheter 31 in a
15 contracted state, and return to an expanded state when it is ejected from lumen 39 of catheter 31 by push tube 34. In this case, the balloon element may be omitted from push tube 34.

Referring to FIGS. 6A and 6B, another
20 alternative embodiment of the stent of the present invention is described. Stent 50 has tubular body 52, exterior surface 54, flange 56 extending radially outward from exterior surface 54, sharpened tip 58, and barbs 60. Bore 62 extends within stent 50 from
25 flange 56 to sharpened tip 58. Apertures 64 enable bore 62 to communicate with exterior surface 54, thereby permitting fluid communication between the interior and exterior of stent 50. Optionally, stent 50 may include aperture 59 in tip 58 that communicates
30 with bore 62, so that when the stent is deployed in myocardium aperture 59 permits flow through bore 62 to pass into an epicardial artery.

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Blood entering bore 62 from the left ventricle enters through flange 56, flows through the bore toward sharpened tip 58, and exits into the myocardium through apertures 64. To promote myocardial angiogenesis, stent 50 is preferably coated on either interior surface 66 or exterior surface 54 with a layer of bioactive agent, as described hereinabove. If optional aperture 59 is also included, the flow through bore 62 may pass into an epicardial artery.

Barbs 60 may comprise wire members, for example, welded to stent 50, that collapse when stent 50 is advanced in the distal direction (i.e., into tissue), but are biased to expand against movement in the proximal direction. Following implantation, barbs 60 extend radially outward from exterior surface 54 to secure stent 50 inside the myocardium and prevent the stent from being ejected into the left ventricle. Although FIG. 6B illustrates four barbs 60, it will be understood by those of ordinary skill in the art that one or more barbs may be used to satisfactorily secure stent 50 in the myocardium.

With respect to FIGS. 7A through 8B, stent 70 is described. Stent 70 comprises tubular body 72, exterior surface 74, proximal tines 76 extending from distal endface 78, conical tip 80, and distal tines 82 recessed in slots 84. Bore 86 extends within stent 70 from distal endface 78 to conical tip 80. Conical tip 80 may, or may not, include an opening that communicates with bore 86. Apertures 88 and slots 84 enable exterior surface 74 to communicate with bore 86, thereby permitting fluid communication between the interior and exterior of stent 70. Tubular body 72 may be coated on either the interior surface or exterior surface 74 with a layer of bioactive agent.

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Distal tines 82 may, for example, comprise wire members welded to stent 70 or may be cut from tubular body 72 when forming slots 84. Distal tines 82 bend within slots 84 when stent 70 is advanced in the distal direction (i.e., into tissue), as illustrated in FIG. 7A, but are biased to deflect radially outward out of slots 84 to engage tissue, thereby resisting movement in the proximal direction, as illustrated in FIG. 8A.

Proximal tines 76 preferably comprise a thermally-activated or pseudo-elastic material, such as a nickel-titanium alloy. Proximal tines 76 have a contracted delivery state, as shown in FIG. 7A, in which they extend parallel to, and in-line with, tubular body 72 (for example, when constrained by delivery sheath 89 shown in dotted line in FIG. 7B). When stent 70 is ejected from the delivery sheath (or the sheath is withdrawn proximally while the stent is held stationary), proximal tines 76 expand radially outward to engage the tissue surface. Thus, for example, in FIGS. 8A and 8B, proximal tines 76 extend radially outward to contact the endocardial surface, thereby preventing further motion in the distal direction.

Accordingly, proximal tines 82 secure stent 70 within the myocardium and prevent the stent from being ejected into the left ventricle, while proximal tines 76 prevent the stent from being urged further into the myocardium by wall motion of the heart. Stent 70 perfuses the myocardium via bore 86 and apertures 88 and slots 84. While FIGS. 7 and 8 illustrate four proximal tines 76 and two distal tines 82, it will be understood by those of ordinary skill in the art that different numbers of such tines may be used to

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satisfactorily secure stent 70 in the myocardium.

In FIG. 9, yet another alternative embodiment of a stent constructed in accordance with the present invention is described. Stent 90 includes first and
5 second tubular members 91 connected by strap 92. Each of tubular members 91 is similar in construction to stent 50 of FIG. 6A, and includes a bore 93 that communicates with exterior surface 94 via apertures 95, and includes barbs 96. Strap 92 couples tubular
10 members 91 to one another and provides further assurance that tubular members 91 will not become dislodged from the tissue and also that the tubular members will not be urged further into the tissue by wall motion of the heart. Alternatively, stent 90 may
15 be formed by bending a hollow, apertured tube into a U-shape to form a staple-like structure.

Referring to FIG. 10, a still further alternative embodiment of a stent constructed in accordance with the present invention is described.
20 Stent 100 comprises tubular body 101 having exterior surface 102, conical tip 103, proximal tines 104 recessed in slots 105 and distal tines 106 recessed in slots 107. Bore 108 extends from distal endface 109 to conical tip 103. Slots 105 and 107 enable exterior
25 surface 102 to communicate with bore 108, thereby permitting fluid communication between the interior and exterior of the stent. Tubular body 101 may be coated on either the interior surface or exterior surface 102 with a layer of bioactive agent, as described
30 hereinabove.

Distal and proximal tines 104 and 106 may, for example, comprise wire members welded to stent 100, or may be cut from tubular body 101 when forming slots 105 and 107, respectively. Distal and proximal tines

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104 and 106 bend within slots 105 and 107,
respectively, when stent 100 is disposed within a
delivery sheath, but are biased to deflect out of slots
105 and 107 to engage the tissue and to resist movement
5 when implanted.

Stent 100 may be implanted, for example,
using the delivery system described hereinafter with
respect to FIGS. 12A and 12B. That delivery system
includes a delivery sheath, push tube and guide wire.
10 In particular, stent 100 may be loaded on the guide
wire so that the proximal end of the stent is in
engagement with the push tube, and so that conical tip
103 extends from the distal end of the sheath. The
stent and catheter are urged against the tissue in
15 which the stent is to be implanted, so that the distal
end of the catheter enters the tissue to a
predetermined depth. The delivery sheath then is
withdrawn proximally while the stent is held stationary
using the push tube. Once the delivery sheath is
20 withdrawn, proximal and distal tines 104 and 106 expand
radially outward to secure the stent in position.

Referring now to FIGS. 11A and 11B, yet
another alternative embodiment of a stent constructed
in accordance with the principles of the present
25 invention is described. Stent 110 comprises tubular
body 111 having exterior surface 112, a plurality of
conical ribs 113, flange 114 and bore 115. Stent 110
may optionally include a series of apertures, not
shown, that extend from bore 115 to the lateral
30 exterior surface 112. The conical rib on the distal-
most endface of stent 110 forms an angle α sufficient
to pierce tissue when a distally-directed force is
applied to flange 114.

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Stent 110 preferably is molded from a bioresorbable material, and is either impregnated or coated with a bioactive agent, as described hereinabove. The distal-most conical rib 113 assists
5 in implanting stent 110, while the proximal faces of the stent prevent it from being ejected into the left ventricle. Flange 114 abuts against the endocardium, when stent 110 is implanted, and prevents further movement of the stent into the myocardium resulting
10 from muscle contraction.

Referring now to FIGS. 12A and 12B, a delivery system for implanting a series of stents 110 in vessel or organ wall is described. Delivery system 120 comprises catheter 121 having distal end 122, first
15 handle portion 123 and second handle portion 124. Delivery system 120 may in addition include a series of stabilization members as described hereinabove for the embodiment of FIGS. 4A and 4B.

As shown in FIG. 12B, distal end 122 of
20 catheter 121 has lumen 125 within which a plurality of stents 110 are engaged end-to-end on wire 126. Push tube 127 engages the proximal face of the proximal-most stent 110 on wire 126, and is engaged at its distal end to second handle portion 124. Second handle portion
25 124 is engaged in first handle portion 123 by threads 128, so that one rotation of second handle portion 124 relative to first handle portion 123 causes push tube 127 to move distally a predetermined distance.

Wire 126 passes through bores 115 of the
30 plurality of stents 110, so that stents 110 may be translated along wire 126 by distal movement of push tube 127. To prevent inadvertent loss of stents 110 from the distal end of wire 126, it may be preferable that stents 110 frictionally engage wire 126 with a

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force that is overcome by push tube 127. Wire 126 includes sharpened tip 129 that assists in piercing tissue to permit implantation of stents 110. Delivery system 120 comprises materials typically employed in catheter manufacture, as described hereinabove.

Delivery system 120 may be inserted into the left ventricle, either percutaneously or intraoperatively, using techniques that are per se known. During insertion of delivery system 120 to a treatment site, the delivery system is manipulated using first handle portion 123, while second handle portion 124 remains in the proximal-most position.

Once distal end 122 of catheter 121 has been disposed at a desired implantation site, for example, as determined by fluoroscopy, first handle portion 123 is urged in the distal direction so that sharpened tip 129 of wire 126 pierces the endocardium. Second handle portion 124 is then rotated a predetermined number of times relative to first handle portion 123 (which is held stationary) so that push tube 127 is translated distally. Push tube 127, in turn, urges one of stents 110 along wire 126 so that the stent becomes implanted in the passage formed by the distal end of wire 126.

In particular, threads 128 may be arranged so that the a predetermined number of rotations of the second handle portion causes stent 110 to become fully implanted, and the next stent 110 in the stack is exposed for implantation at a subsequent implantation site. Delivery system 120 is then retracted proximally and repositioned to a new implantation site. When fully implanted, flange 114 of stent 110 abuts against the endocardium, while conical ribs 113 prevent movement of the stent in a proximal direction. Delivery system 120 advantageously enables a number of

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stents to be implanted during a single insertion of the delivery system to the treatment site.

In FIG. 13, a yet further embodiment of a stent constructed in accordance with the present invention is described. Stent 130 comprises body 131 formed of a series of conical sections 132, and includes a bore (not shown) that communicates with apertures 133 in lateral exterior surface 134. Distal-most conical section 132 includes sharpened tip 135.

When implanted in the myocardium, blood from the left ventricle enters the bore through an inlet (not shown) in proximal-most conical section 132, flows through the bore toward sharpened tip 135, and exits into the myocardium through apertures 133 in the manner described hereinabove with respect to the embodiment of FIG. 1. Stent 130 may be constructed as described hereinabove.

Stent 130 may be implanted with a delivery system similar to that described in FIGS. 12A and 12B. Instead of having the stents arranged on wire 126, however, stents 130 may be stacked within the lumen of a catheter in a nested fashion, i.e., so that tip 135 of one stent is engaged in the inlet of the bore of the next distal-most stent in the stack. The proximal-most stent in the stack engages a push tube which may be similar in construction to push tube 127 of delivery system 120.

To prevent the stents from falling out inadvertently, for example, while positioning the delivery system, edges 136 of the stents may be frictionally engaged with the inner surface of the lumen with a force that is sufficiently low to be overcome by the push tube. In this manner, a series of stents may be implanted at selected positions within a

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vessel or organ wall, without having to repeatedly reload the delivery system.

With respect to FIGS. 14A to 14D, a yet further alternative embodiment of a stent of the present invention is described. Stent 140 comprises a tubular member 141 having spring-biased barbs 142 and 143 and sharpened tip 144. Tubular member 141 may include a bore (not shown) extending from its proximal to distal ends to enhance perfusion. Tubular member 141 preferably comprises a bioresorbable material, such as described hereinabove, and preferably is impregnated with a bioactive substance to stimulate revascularization and/or tissue regeneration.

Barbs 142 and 143 preferably have a contracted delivery state, wherein the ends of the barbs lie parallel to (or recessed in) exterior surface 145 of the stent, as shown in FIG. 14A, and a deployed state, wherein the ends of the barbs extend radially outward, as shown in FIG. 14B. Barbs 142 and 143 preferably are arranged with the free ends directed in opposing relation, so as to secure stent 140 against movement once implanted. Stents 140 may be implanted percutaneously, for example, using the delivery system of FIGS. 12A and 12B.

In FIG. 14C, tubular member 150 suitable for use in constructing stent 140 has a physical or chemical property that varies along the length of the member from proximal end 151 to distal end 152, as indicated by the density of the shading in FIG. 14C. For example, tubular member 150 may be biodegradable, and have a lower density at the proximal end than at the distal end, so that the tubular member erodes in the direction shown by arrow A. Alternatively, tubular member 150 may be impregnated with a drug, or other

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bioactive agent, that elutes in a higher concentration from the distal end of the tubular member than from the proximal end.

In FIG. 14D, stent 153 having a tubular member similar to that of stent 140 of FIGS. 14A and 14B is shown in cross-section. Instead of having a property that varies as a function of length, like the embodiment of FIG. 14C, stent 153 has a property that varies as a function of radial thickness. Specifically, stent 153 comprises three concentric layers of different growth factors 154, 155 and 156, respectively. Stent 153, which preferably comprises a bioerodible or elutable material, therefore enables a sequence of bioactive agents to be delivered to myocardial tissue over a period of time.

Referring now to FIG. 15, a further alternative embodiment of the stent of FIGS. 14 is described for intraoperative use. Stent 160 comprises tubular member 160 formed of a bioresorbable material, and impregnated with a bioactive agent. Stent 160 may have a length of from 3 to 100 mm, and is expected to stimulate revascularization when intraoperatively implanted adjacent to a stenosed artery.

In particular, during an intraoperative procedure, for example, a bypass grafting procedure, a channel first is formed in epicardium EP at a position adjacent to cardiac artery CA having stenosis S. Stent 160 is then inserted into the channel, and may be secured with sutures 162. Stent 160 elutes a bioactive agent, such as described hereinabove, into the surrounding tissue. It is expected that the bioactive agent will encourage revascularization, including the growth of new networks of capillaries C, that provide blood to the tissue downstream of stenosis S.

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Although preferred illustrative embodiments of the invention are described above, it will be apparent to one skilled in the art that various changes and modifications may be made therein without departing
5 from the invention, and the appended claims are intended to cover all such changes and modifications that fall within the true spirit and scope of the invention.

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What Is Claimed Is:

1. A stent suitable for implantation in myocardial tissue to enhance perfusion therein, the stent comprising:

a tubular member having first and second ends, the first end configured to pierce myocardial tissue; and

means for retaining the tubular member within the myocardial tissue.

2. The stent as defined in claim 1 further comprising a bioactive agent.

3. The stent as defined in claim 1 wherein tubular member further includes a portion defining a bore extending longitudinally from the second end and a plurality of apertures extending from the bore to an exterior lateral surface of the stent.

4. The apparatus as defined in claim 1 wherein the tubular member further comprises a bore extending longitudinally from the first end to the second end.

5. The stent as defined in claim 3 wherein the first end further comprises a portion defining an opening that communicates with the bore.

6. The stent as defined in claim 1 wherein the means for retaining comprises a flange that abuts against an endocardial tissue surface.

7. The stent as defined in claim 6 wherein the means for retaining comprises a plurality of tines

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having a delivery state, wherein the plurality of tines are retracted against an exterior surface of the stent, and a deployed state, wherein the plurality of tines extend radially outward from the exterior surface to engage the myocardial tissue.

8. The stent as defined in claim 6 wherein the means for retaining comprises a plurality of tines having a delivery state, wherein the plurality of tines are retracted within slots formed in an exterior surface of the stent, and a deployed state, wherein the plurality of tines extend radially outward from the exterior surface to engage the myocardial tissue.

9. The stent as defined in claim 2 wherein the tubular member has an exterior surface and the bioactive agent comprises a layer of material disposed on the exterior surface.

10. The stent as defined in claim 2 wherein the bore has an interior surface and the bioactive agent comprises a layer of material disposed on the interior surface.

11. The stent as defined in claim 1 wherein the tubular member comprises a bioresorbable material.

12. The stent as defined in claim 11 wherein the bioresorbable material is impregnated with the bioactive agent.

13. The stent as defined in claim 12 wherein the bioresorbable material further includes a physical or chemical property that varies from the first end to

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the second end.

14. The stent as defined in claim 12 wherein the bioresorbable material further includes a physical or chemical property that varies from as a function of the thickness of the stent.

15. The stent as defined in claim 1 wherein the means for retaining comprises a radially expandable mesh portion of the tubular member.

16. The stent as defined in claim 15 wherein the radially expandable mesh is permanently deformable.

17. The stent as defined in claim 15 wherein the radially expandable mesh is self-expanding.

18. The stent as defined in claim 1 wherein the means for retaining comprises at least one barb projecting from an exterior surface of the tubular member.

19. The apparatus as defined in claim 1 wherein the means for retaining comprises a plurality of conical ribs.

20. The apparatus as defined in claim 1 wherein the first end of a first stent is configured to nest within a second end of a second stent.

21. The apparatus as defined in claim 2 wherein the bioactive agent comprises an angiogenic growth factor selected from the group consisting of VEG-F, FGF type I and FGF type II.

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22. A method of implanting a stent within myocardial tissue to enhance perfusion therein, comprising:

providing a stent comprising a tubular member having first and second ends, the first end configured to pierce myocardial tissue, and means for retaining the tubular member within the myocardial tissue;

positioning the first end of the stent at a desired implantation site;

applying force to the second end of the stent to implant the stent within the myocardial tissue; and

engaging the means for retaining with the myocardial tissue to retain the stent in position.

23. The method as defined in claim 22 further comprising:

stimulating revascularization or tissue regeneration using a bioactive agent eluted from the stent.

24. The method as defined in claim 22 wherein the tubular member further comprises a flange projecting from the second end, the method further comprising:

when the flange abuts against an endocardial tissue surface, ceasing application of force to the second end of the stent.

25. The method as defined in claim 22 wherein the means for retaining comprises a plurality of tines or barbs having a contracted delivery state and a deployed state, the method further comprising:

delivering the tubular member to an implantation site within a delivery sheath with the

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plurality of tines or barbs in the contracted delivery state; and

retracting the delivery sheath to enable the plurality of tines or barbs to expand to the deployed state to secure the stent within the myocardial tissue.

26. The method as defined in claim 22 wherein the means for retaining comprises an expandable mesh portion, and engaging the means for retaining with the myocardial tissue comprises expanding the expandable mesh portion to secure the stent in position within the myocardial tissue.

27. The method as defined in claim 22 wherein positioning the first end of a stent at an implantation site comprises:

providing a delivery system;

loading the stent into the delivery system;

and

inserting the delivery system percutaneously to position the first end of a stent at an implantation site.

28. The method as defined in claim 27 wherein the tubular member comprises a bore having an inlet end and an outlet end, and wherein applying force to the second end of the stent to implant the stent within the myocardial tissue causes the outlet end to pierce an epicardial artery, so that blood passes through the bore from a cardiac chamber and into an epicardial artery.

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29. The method as defined in claim 22 wherein positioning the first end of a stent at an implantation site comprises:
providing a delivery system;
loading the stent into the delivery system;
and
inserting the delivery system intraoperatively to position the first end of a stent at an implantation site.

30. A method of implanting a stent within myocardial tissue to enhance perfusion therein, comprising:
providing a stent comprising a tubular member having first and second ends, the stent comprising a bioresorbable material impregnated with a bioactive agent;
forming a channel in the myocardial tissue at a desired implantation site; and
inserting the stent within the channel to stimulate revascularization or tissue regeneration.

31. The method as defined in claim 30 further comprising:
eluting the bioactive agent from the bioresorbable material.

32. The method as defined in claim 31 further comprising:
securing the stent within the channel by applying sutures.

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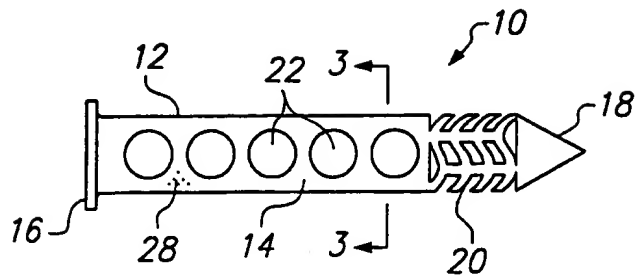


FIG. 1

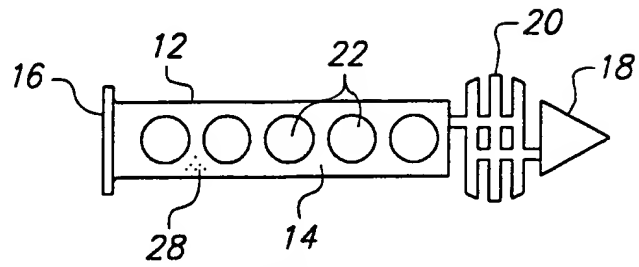


FIG. 2

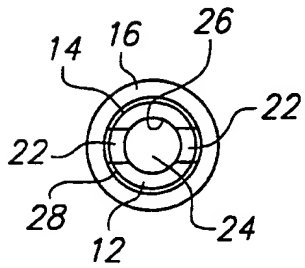


FIG. 3

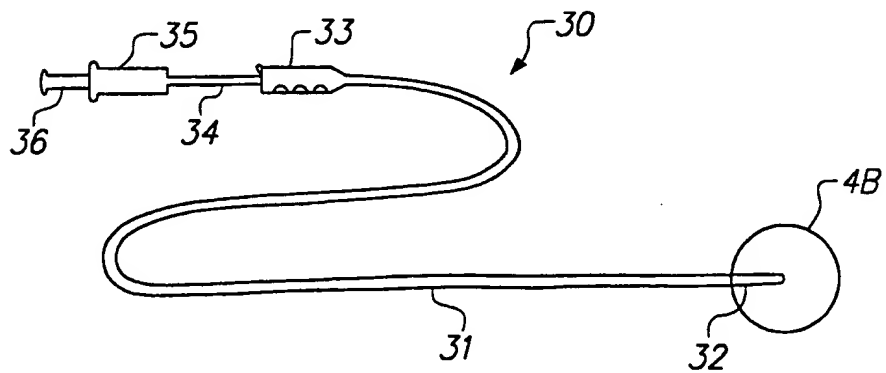


FIG. 4A

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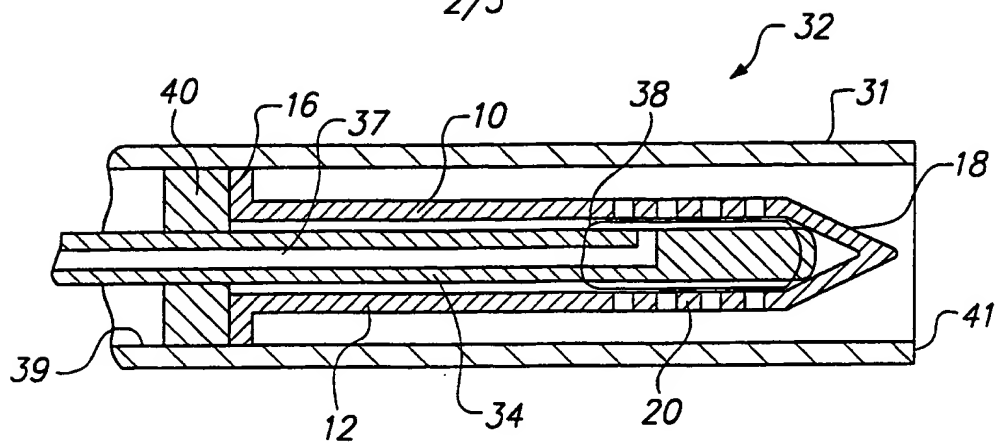


FIG. 4B

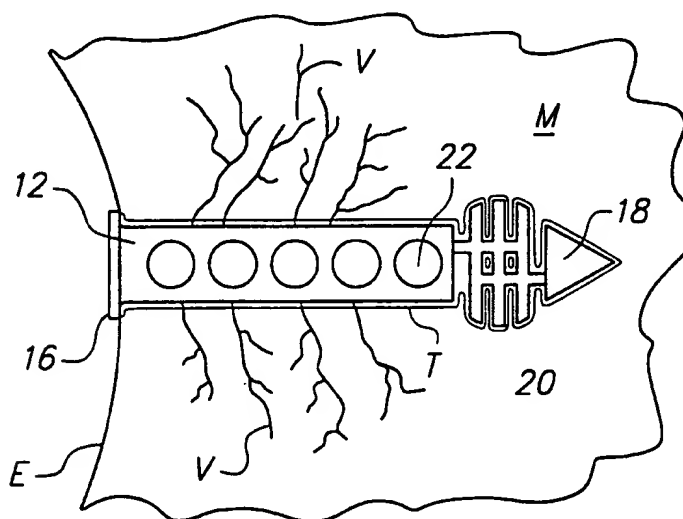


FIG. 5

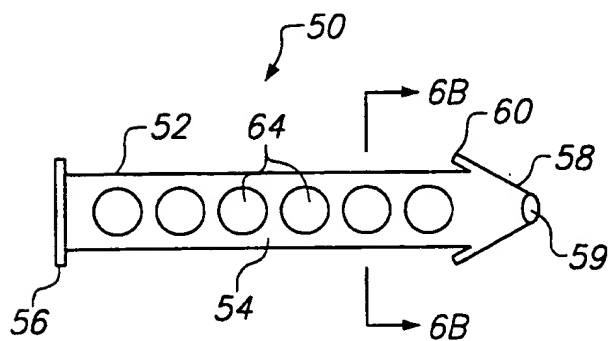


FIG. 6A

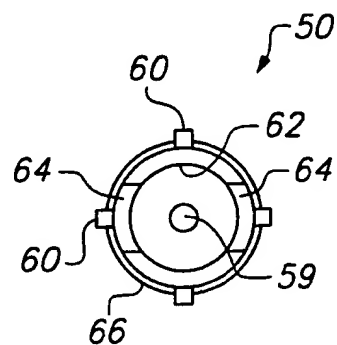


FIG. 6B

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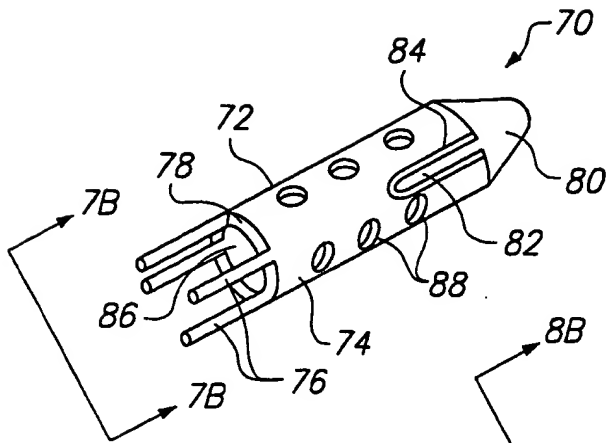


FIG. 7A

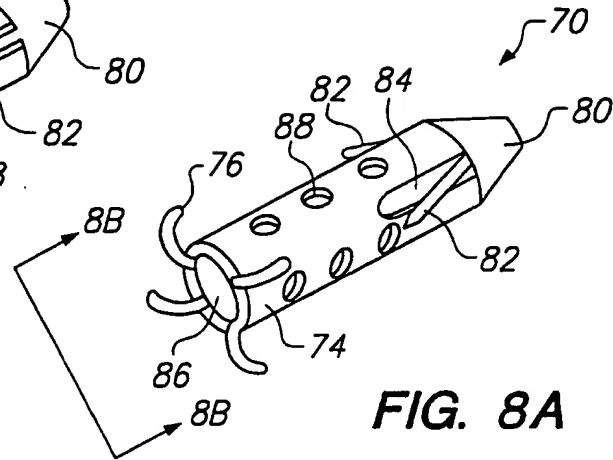


FIG. 8A

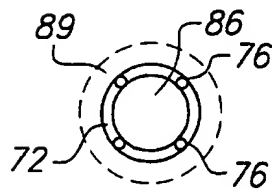


FIG. 7B

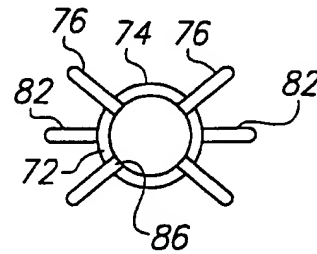


FIG. 8B

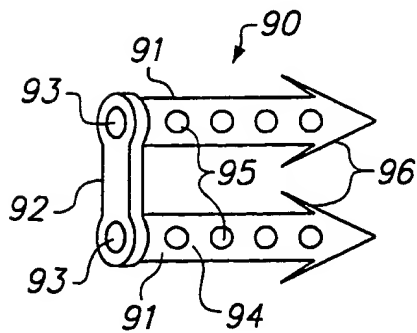


FIG. 9

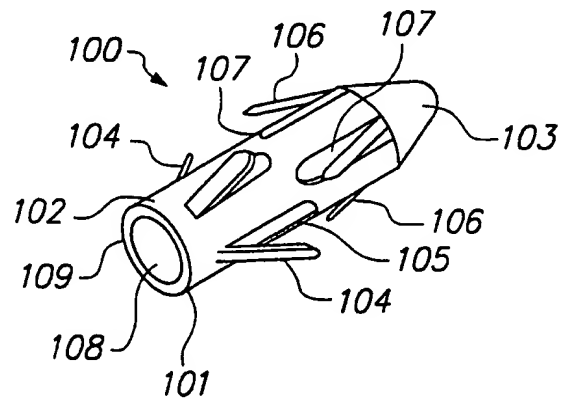


FIG. 10

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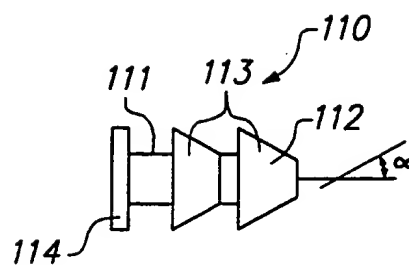


FIG. 11A

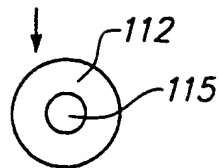


FIG. 11B

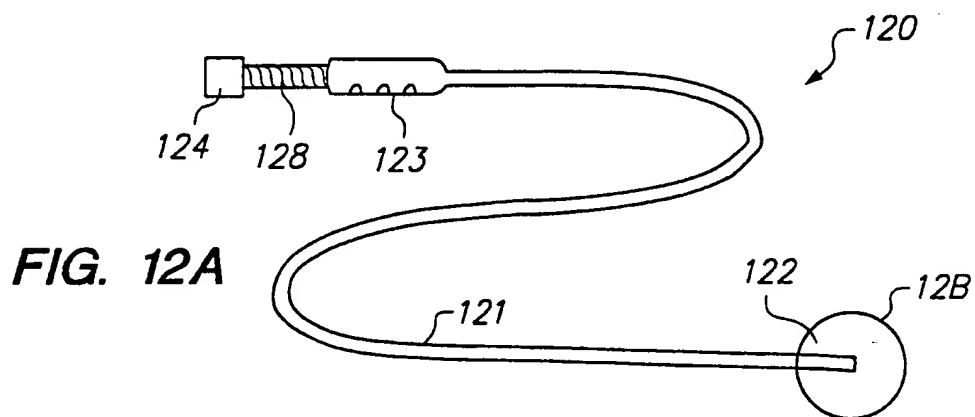


FIG. 12A

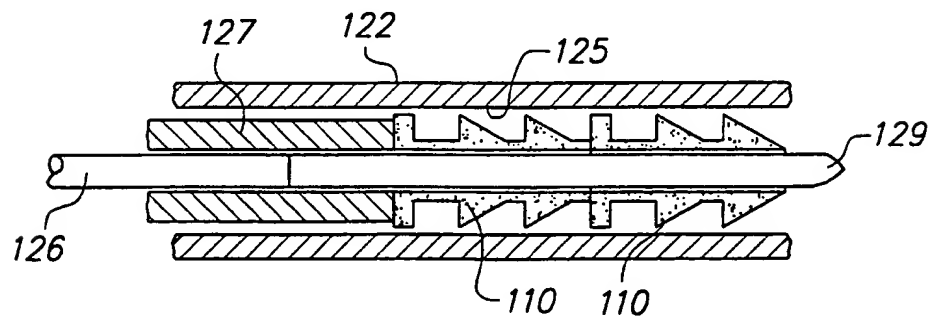


FIG. 12B

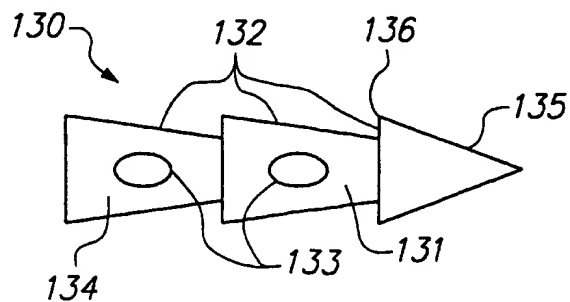


FIG. 13

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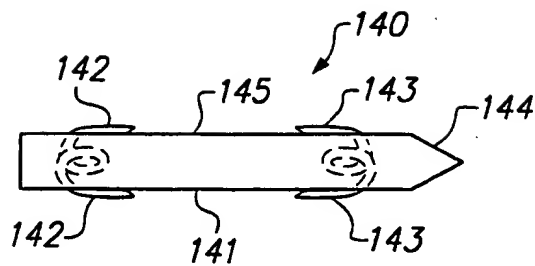


FIG. 14A

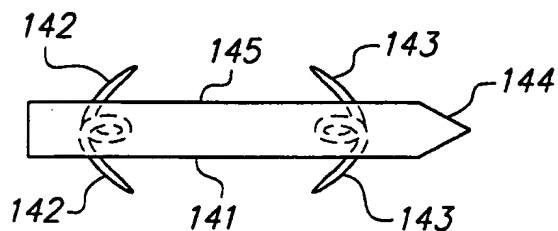


FIG. 14B

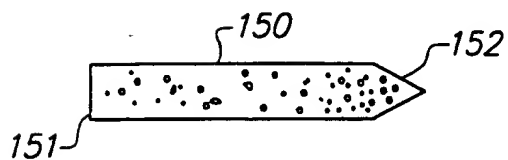


FIG. 14C

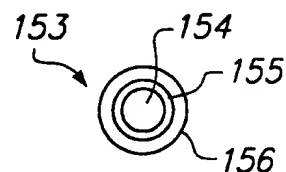


FIG. 14D

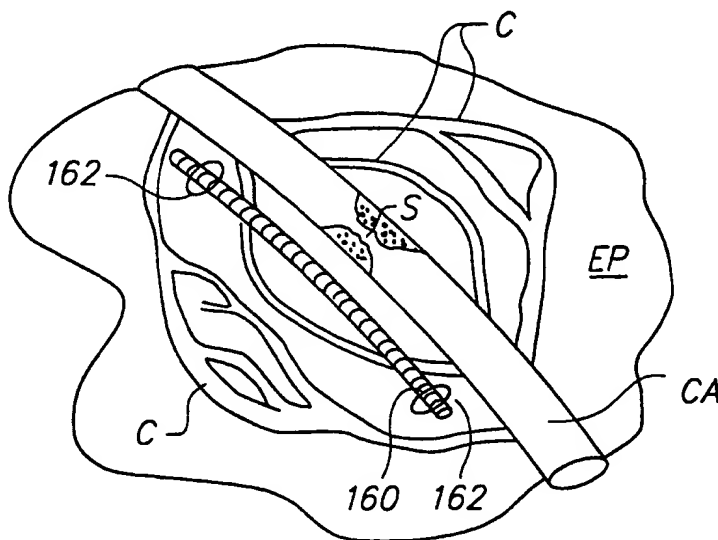


FIG. 15

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US99/30118

A. CLASSIFICATION OF SUBJECT MATTER

IPC(7) :A61F 02/06

US CL :623/1; 606/198

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 606/191, 192, 194, 198; 623/1, 11, 12

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	US 5,059,211 A (STACK) et al. 22 October 1991, entire document.	11-14
Y	US 5,342,348 A (KAPLAN) 30 August 1994, entire document.	22-32
X	US 5,617,878 A (TAHERI) 08 April 1997, entire document.	1, 3-8, 15, 16, 18, 20, 22, 24, 26, 27, 29
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Y		2, 9-14, 23, 30- 32
X	US 5,681,345 A (EUTENEUER) 28 October 1997, entire document.	1, 15, 17

☒ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

* Special categories of cited documents:	*T* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
A document defining the general state of the art which is not considered to be of particular relevance	*X* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
E earlier document published on or after the international filing date	*Y* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
L document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	*Z* document member of the same patent family
O document referring to an oral disclosure, use, exhibition or other means	
P document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search 24 MARCH 2000	Date of mailing of the international search report 25 MAY 2000
Name and mailing address of the ISA/US Commissioner of Patents and Trademarks Box PCT Washington, D.C. 20231 Facsimile No. (703) 305-3230	Authorized officer GLENN K. DAWSON Telephone No. (703) 308-4304

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US99/30118

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	US 5,707,385 A (WILLIAMS) 13 January 1998, entire document.	2, 9, 10, 12-14, 21
Y,P	US 5,899,917 A (EDWARDS et al.) 04 May 1999, entire document.	22-32
Y	WO 97/32551 A (HUSSEIN et al.) 12 September 1997, entire document.	22-32

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